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## Understanding wasted/ineffective efforts in mechanically ventilated COPD patients using the Campbell diagram

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### Electronic supplementary material

The online version of this article (doi:10.1007/s00134-008-1095-7) contains supplementary material, which is available to authorized users.

This physiological note is accompanied by Electronic Supplementary Material containing a Powerpoint presentation. This is an independent Powerpoint presentation that has a structured animation of ventilator waveforms exhibiting wasted efforts and the use of the Campbell diagram to understand wasted efforts in COPD. It is thus accompanied by notes beneath each slide so that the reader can go through the presentation without referring to the text.

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### Introduction

Wasted or ineffective efforts are inspiratory efforts that fail to trigger the ventilator [1]. Nearly 25% of mechanically ventilated patients exhibit ineffective efforts which are even more frequent in COPD patients [2]. The pathophysiology of wasted efforts can be illustratively presented using the Campbell diagram.

### Campbell diagram

The Campbell diagram is constructed by plotting the dynamic relation between pleural pressure (measured with an esophageal balloon) and lung volume during breathing in relation to the passive pressure-volume curves of the lung  $P_{el}(L)$  and the chest wall  $P_{el}(cw)$  [3]. The  $P_{el}(cw)$  is constructed by connecting the values taken by the esophageal pressure during passive inflation (i. e., with no respiratory muscle activity) at different lung volumes; thus, any change in esophageal pressure is referred to this line in the Campbell diagram in order to calculate the true muscular pressure developed by the patient.

In normal subjects inspiration starts from the relaxation volume of the respiratory system ( $V_r$ ), where the  $P_{el}(L)$  and  $P_{el}(cw)$  intersect (i. e., where the tendency of the lung to recoil inward is equal to the tendency of the chest wall to expand; Fig. 1a). Inspiratory muscle action results in pressure development ( $P_{insp}$ ) on the left of the  $P_{el}(cw)$ . Inspiratory flow, and thus increases in volume ( $V_L$ ), take place on the left of the  $P_{el}(L)$  and coincide with the beginning of inspiratory muscle action. At any volume, the horizontal distance between the  $P_{el}(cw)$  and  $P_{el}(L)$  represents the portion of inspiratory muscle action devoted to expanding the lung at this volume with open airways and the portion on the left of the  $P_{el}(L)$  represents the pressure dissipated to generate airflow. Inspiration ends on the  $P_{el}(L)$  (point of zero flow) and the inspiratory muscles relax [so that pressure returns on the  $P_{el}(cw)$ ]. Expiration is usually passive, and the respiratory system returns to its relaxation volume on the  $P_{el}(cw)$ ; however, in patients with respiratory distress, such as mechanically ventilated COPD patients, expiration is frequently active. In the case of active expiration, pressure develops on the right of the  $P_{el}(cw)$  due to activity of expiratory muscles ( $P_{exp}$ ). This returns volume back to the relaxation volume of the respiratory system.

**Why are COPD patients prone to develop wasted/ineffective efforts?**

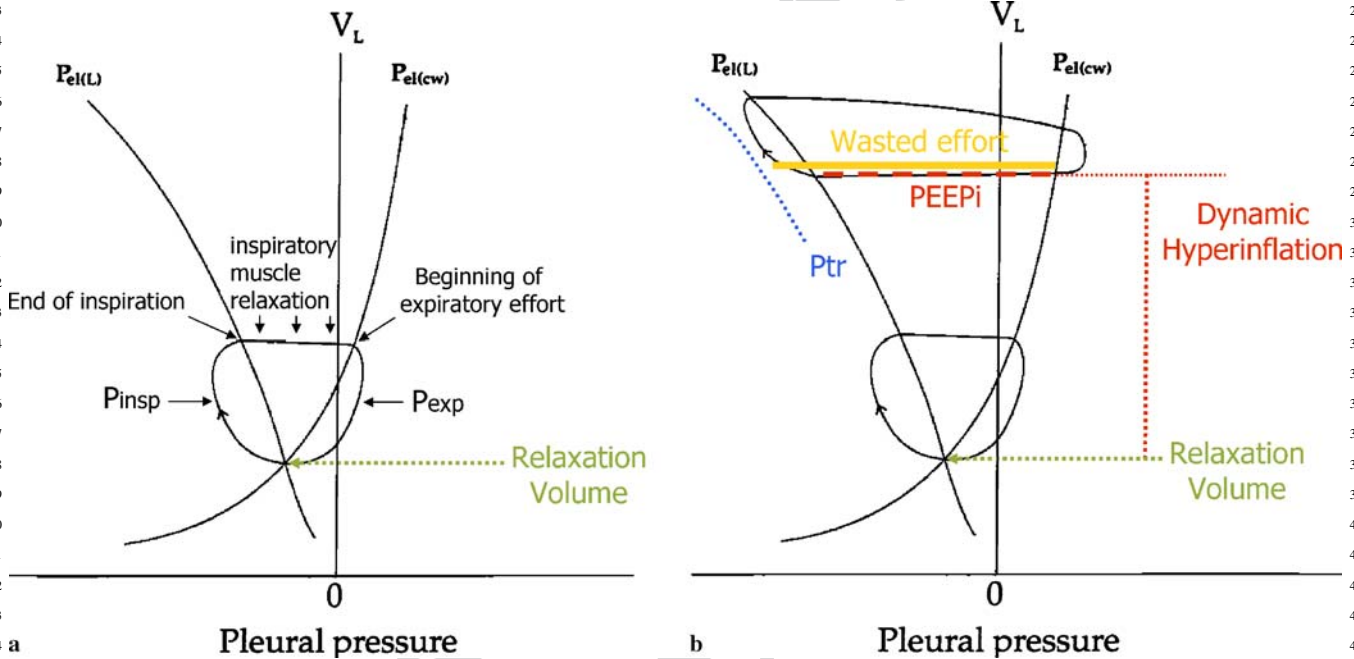
In COPD patients with dynamic hyperinflation, inspiration starts from an increased end-expiratory lung volume (Fig. 1b). Inspiratory muscle action has to overcome the intrinsic positive end expiratory pressure [PEEPi, horizontal distance between the  $P_{el(L)}$  and  $P_{el(cw)}$ ] before it results in inspiratory flow and thus increases in volume ( $V_L$ ). In mechanically ventilated patients, inspiratory muscle action has to additionally overcome the trigger sensitivity (Ptr) of the ventilator [horizontal distance between the  $P_{el(L)}$  and Ptr] before it results in inspiratory flow and thus increases in volume ( $V_L$ ); thus, in mechanically ventilated COPD patients, inspiratory muscle action has to overcome PEEPi plus the trigger sensitivity (Ptr).

When the magnitude of inspiratory muscle action is less than the sum of PEEPi plus Ptr this inspiratory effort

cannot trigger the ventilator, and thus does not result in inspiratory flow and thus increases in volume ( $V_L$ ). This inspiratory effort is called ineffective or wasted.

**Is the Campbell diagram useful for estimating the work of breathing during wasted efforts?**

The Campbell diagram is useless to estimate inspiratory work of breathing when inspiratory triggering does not happen (i. e., during wasted efforts): work is physically defined as the area subtended in a pressure/volume loop. Since there is no inspiratory volume, the work is zero (albeit muscles, indeed, consume energy). The energy expenditure during non-triggered wasted inspiratory efforts can be estimated by the pressure/time product: the product of the pressure developed by the inspiratory muscles [difference between the measured esophageal



**Fig. 1 a** In normal subjects inspiration starts from the relaxation volume of the respiratory system, where the passive pressure-volume curves of the lung [ $P_{el(L)}$ ] and chest wall [ $P_{el(cw)}$ ] intersect. Inspiratory muscle action results in pressure development ( $P_{insp}$ ) on the left of the pressure-volume curve of the chest wall [ $P_{el(cw)}$ ]. Inspiratory flow, and thus increases in volume ( $V_L$ ) take place on the left of the pressure-volume curve of lung and coincide with the beginning of inspiratory muscle action. Inspiration ends on the pressure-volume curve of the lung and the inspiratory muscles relax (so that pressure returns on the pressure-volume curve of the chest wall). In the case shown, expiration is active so that pressure develops on the right of the pressure-volume curve of the chest wall due to activity of expiratory muscles ( $P_{exp}$ ). This returns volume back to the relaxation

volume of the respiratory system. **b** In COPD patients with dynamic hyperinflation, inspiration starts from an increased end-expiratory lung volume. Inspiratory muscle action has to overcome the intrinsic positive end expiratory pressure [PEEPi, red dashed line, horizontal distance between the  $P_{el(L)}$  and  $P_{el(cw)}$ ] before it results in inspiratory flow and thus increases in volume. In mechanically ventilated patients, inspiratory muscle action has to overcome PEEPi plus the trigger sensitivity (Ptr) before it results in inspiratory flow and thus increases in volume ( $V_L$ ). When the magnitude of inspiratory muscle action is less than the sum of PEEPi + Ptr this inspiratory effort (orange line) cannot trigger the ventilator and consequently does not result in inspiratory flow and thus increases in volume ( $V_L$ ). This inspiratory effort is called ineffective or wasted.

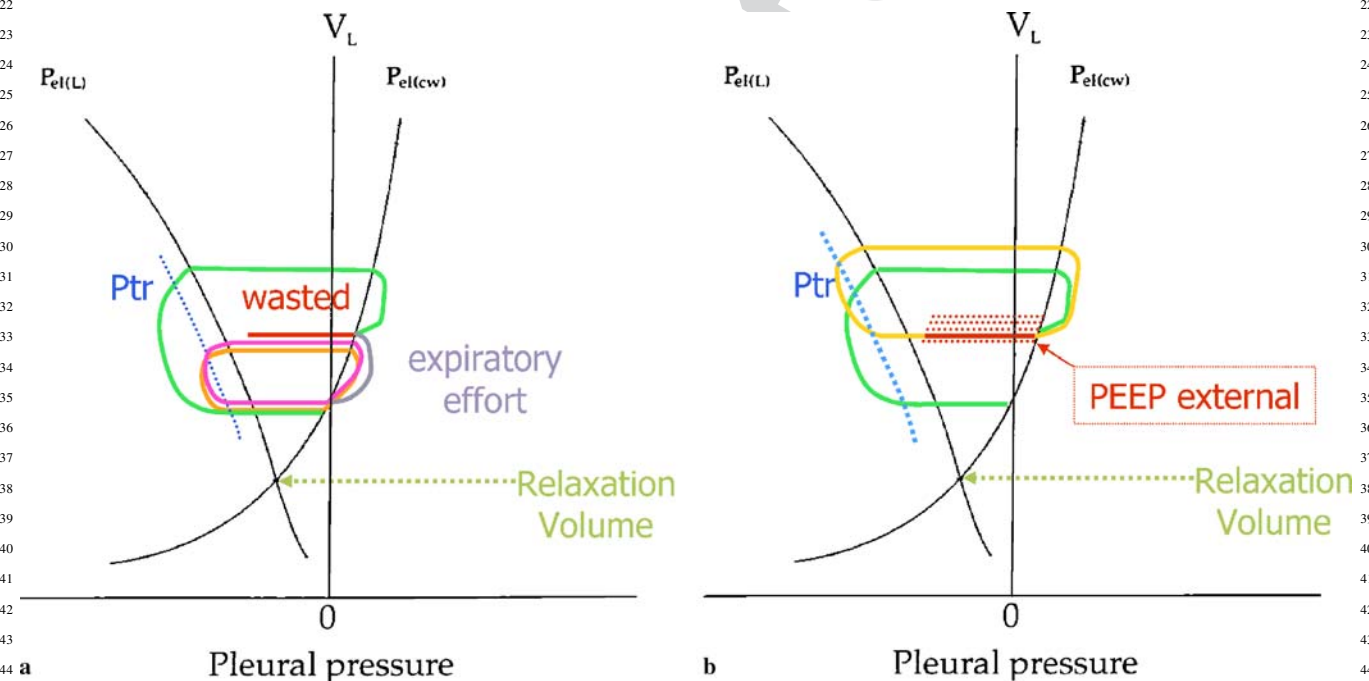
1 pressure and the  $P_{el}(cw)$ ] multiplied by the time of muscle  
 2 contraction (i. e., neural  $T_i$ ).

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 5 **How are ventilator settings affecting the incidence**  
 6 **of wasted/ineffective efforts?**  
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 9 Excessive ventilator support predisposes to ineffective ef-  
 10 forts irrespective of the mode used [2, 4–7]. This is be-  
 11 cause, in the case of COPD, excessive pressure or vol-  
 12 ume delivered by the ventilator combined with the long  
 13 time constant of the respiratory system (which retards lung  
 14 emptying) and/or a short imposed expiratory time (in case  
 15 of volume or pressure control) results in further increased  
 16 end-expiratory lung volume before the next inspiratory ef-  
 17 fort begins (Fig. 2a, green curve). At the same time, ex-  
 18 cessive ventilator assistance reduces inspiratory muscle ef-  
 19 fort, via either a phenomenon called neuromechanical in-  
 20 hibition (the main mechanism most likely being the Her-  
 21 ing–Breuer reflex) [8], and/or by producing alkalemia via

1 excessive  $CO_2$  reduction in patients with chronic bicarbon-  
 2 ate elevation, thus reducing the drive to breathe [2]. The  
 3 ensuing inspiratory effort is inadequate to overcome PEEP<sub>i</sub>  
 4 plus  $P_{tr}$  and thus, this inspiratory effort fails to trigger the  
 5 ventilator (Fig. 2a, red line  $\square$ ). This is of course exagger-  
 6 ated in the presence of respiratory muscle weakness [7].  
 7 The following expiratory effort (Fig. 2a, blue curve) de-  
 8 creases the end expiratory lung volume. When the end ex-  
 9 piratory lung volume decreases to a level where the ensu-  
 10 ing inspiratory effort exceeds PEEP<sub>i</sub> plus  $P_{tr}$ , the ventila-  
 11 tor is triggered again to deliver a machine breath (Fig. 2a,  
 12 mauve curve). The breath-to-breath variability in breathing  
 13 pattern contributes to the variability in the end-expiratory  
 14 lung volume and thus to the frequency of ineffective ef-  
 15 ferts [7].

16 Alternatively, during assist control mechanical venti-  
 17 lation, prolonged imposed inspiratory time (machine  $T_i$ )  
 18 greater than the patient's neural  $T_i$  results in a situation  
 19 where the ventilator is inflating the patient long after the in-  
 20 spiratory muscles have stopped their contraction, i. e., dur-  
 21 ing the neural expiration [6, 9]. During pressure support



46 **Fig. 2 a** In the case of COPD presented, the first inspiratory effort  
 47 (orange curve) triggers the ventilator. In the next breath that trig-  
 48 gered the ventilator, excessive ventilator assistance (either pressure  
 49 or volume) resulted in large tidal volume (green curve), which  
 50 combined with the long time constant of the respiratory system  
 51 (which retards lung emptying) and/or a short imposed expiratory  
 52 time (in case of volume or pressure control) led to further increased  
 53 end-expiratory lung volume before the next inspiratory effort  
 54 begins (green curve). The ensuing inspiratory effort is inadequate  
 55 to overcome PEEP<sub>i</sub> +  $P_{tr}$  due to the increased end expiratory lung  
 56 volume; thus, this inspiratory effort fails to trigger the ventilator  
 (wasted or ineffective effort, red line). The following expiratory  
 effort (blue curve) decreases the end-expiratory lung volume. When

the end-expiratory lung volume decreases to a level where the  
 ensuing inspiratory effort exceeds PEEP<sub>i</sub> +  $P_{tr}$ , the ventilator is  
 triggered again to deliver a machine breath (mauve curve). **b** In the  
 presence of increased end-expiratory lung volume (green curve),  
 addition of an amount of external PEEP lower than the intrinsic  
 PEEP (red dotted lines) offers part of the pressure required to  
 overcome PEEP<sub>i</sub> +  $P_{tr}$ . The inspiratory effort starts closer to the  
 passive pressure-volume curve of the lung [ $P_{el}(L)$ ]. The horizontal  
 distance between this point and the passive pressure-volume curve  
 of the chest wall [ $P_{el}(cw)$ ] is the applied PEEP (PEEP external).  
 The inspiratory effort is now adequate to trigger the ventilator  
 (orange curve)

ventilation, the expiratory trigger threshold (percentage of peak inspiratory flow at which the ventilator cycles to expiration) might be quite low, leading to pressure support being delivered well beyond the patient's neural Ti [10]. In either case, the next inspiratory effort (controlled by the patient's respiratory controller) begins during the early phase of ventilator expiration, i. e., at an increased lung volume [5]. This effort might not be sufficient to overcome PEEPi plus Ptr, and thus this inspiratory effort also fails to trigger the ventilator.

### How can wasted efforts be detected at the bedside?

Wasted efforts can be clinically detected when the breaths delivered by the ventilator (measured rate on the ventilator display) are less than the number of inspiratory efforts of the patient (on clinical examination) at the same time interval (see ESM, slides 1 and 2). On modern ventilator screens, ineffective efforts can be detected as abrupt airway pressure drop simultaneous to an abrupt decrease in expiratory flow (from the flow trajectory established earlier during expiration) and not followed by a machine breath (see ESM, slide 2). Monitors that can automatically detect wasted efforts are under clinical testing and will become available in the future [11, 12].

### What ventilator adjustments should be done in the presence of wasted/ineffective efforts?

The self-evident solution to reduce the frequency of wasted efforts is to decrease the level of excessive ventilator assistance, thus reducing hyperinflation and the pathophysiol-

ogy presented above [4, 6, 7]; however, this might not be always clinically feasible, since it might lead to respiratory distress and to derangement of blood gases [6].

Another solution is the use of PEEP [1, 6]. The addition of an amount of external PEEP lower than the intrinsic PEEP (Fig. 2b, red dotted lines) offers part of the pressure required to overcome PEEPi plus Ptr (Fig. 2b). The inspiratory effort starts closer to the Pel(L) [the horizontal distance between this point and the [Pel(cw) being the applied PEEP (PEEP external)]. The inspiratory effort is now adequate to trigger the ventilator (orange curve).

During assist control reducing machine Ti (or equivalently increasing the inspiratory flow) may prevent ventilator delivery beyond the patients' neural Ti and will reduce wasted efforts. Similarly, during pressure support increasing the expiratory trigger threshold will stop the breath earlier and will reduce wasted efforts [13].

### Conclusion

Wasted efforts are a major cause of patient ventilator dyssynchrony that increase the energy expenditure of the respiratory muscles and may injure them. Understanding their pathophysiology is essential to properly adjust the ventilator settings to attenuate or eliminate them. Wasted efforts should be searched before any change in ventilator settings is implemented during assisted modes of mechanical ventilation, since any ensuing increase in ventilator rate might be caused by the attenuation of wasted efforts (the ventilator rate now approaching the patient's respiratory controller rate) and not by the development of respiratory distress with the new settings.

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